

Design of Low Power Neuro-amplifier Circuit with Miller Compensation Technique for Biomedical Neuro-implantable Devices

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Abstract

Neuro-amplifiers form an integral part of biomedical implantable devices. In this paper, we design a neuro-amplifier circuit with Miller compensation capacitor. The neuro-amplifier design is based on operational transconductance amplifier (OTA) with an active load. In this work, performance of the neuro-amplifier is enhanced by incorporating the Miller compensation technique. Design and simulation of the neuro-amplifier circuit is performed using SPICE simulation software. Body biasing and feedback techniques are imparted to optimize the circuit performance. Simulation results show that the neuro-amplifier circuit has a mid-frequency gain and 3-dB bandwidth of 48dB, and 16kHz respectively.

Keywords: Neuro-implantable device, neuro-amplifier, operational transconductance amplifier (OTA), bio-medical, Miller compensation.

1 Introduction

In recent times, much focus has been on developing implantable biomedical devices for health-care applications [1-2]. A typical biomedical device constitutes sensor modules like chemical/biological sensors [3-11], thermal sensors [12], pressure sensors [13-14], signal processing units like wireless power units [15-16], rectifier [17-18], amplifier [19-20], regulator [21], etc., to mention a few. Typically, the sensor and actuator modules are realized with micro-electro-mechanical systems (MEMS) technology. On the other hand, the signal processing elements are realized with conventional CMOS integrated circuit (IC) technology. Amongst various applications, development of neuro-implants for brain computer interfacing (BCI) is a challenging task especially due to its stringent performance metrics. Biomedical devices for monitoring neural activities have been the focus of research mainly for addressing issues related to neural disorders [22-23]. There are various sub-units that constitute a biomedical device for detecting neural signals. Neural activities are monitored with MEMS based multi-electrode arrays [24]. Apart from neural stimulation [22-25], the other applications include recording and amplification of the analog neural signals using a neuro-amplifier [26-27]. The neural amplifier amplifies the action potential (AP) and local field potentials (LPF). Wireless modules are also typically integrated not only for wireless power transfer but also for signal transmission. Power supply transferred wirelessly is processed with power rectifier and AC-DC converter circuits. This regulated DC supply is used by other circuits in the IC. Wireless power transfer technique typically realized by using inductive coupled links has advantages such as effective silicon estate utilization due to elimination of on-chip battery, high efficiency, improved device life time, to mention a few.

Design of the aforementioned building blocks is challenging, especially due to the stringent power budget in an IC and its trade-off with various performance metrics. In this paper, we investigate the design of a neuro-amplifier-a operational transconductance amplifier (OTA). Design and implementation of the circuits is performed using SPICE software.



2 Architecture and circuit topologies

The general architecture of a bio-implantable device is shown in Fig 1. Various modules in a bio-implantable device include the following: (i) wireless power transfer module, (ii) power rectifier, (iii) neuro-amplifier, (iv) neural simulator and (v) signal processing and communication module.

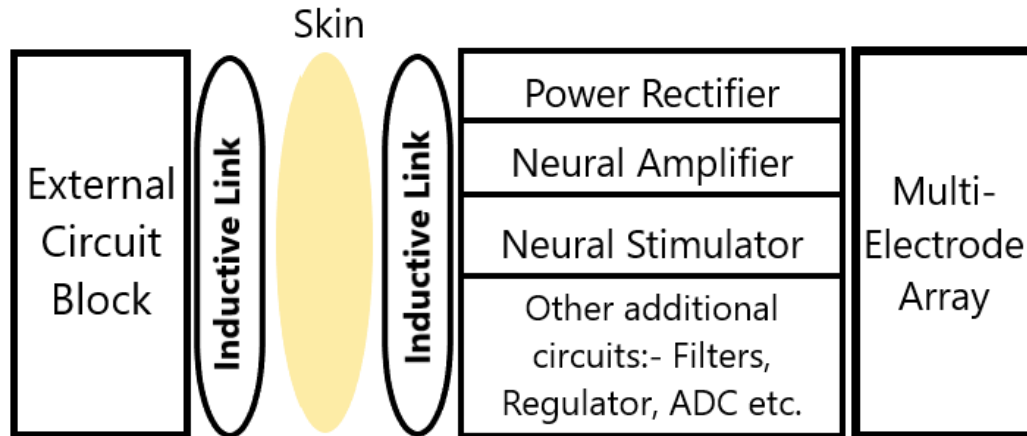


Fig. 1. Block diagram of a general implantable device and its components.

Typically, a bio-implantable device gauges neural activity with micro-electrode sensor arrays followed by amplification of neural signals using a neuro-amplifier. Subsequently, neuro-amplifier output undergoes digital signal processing so that it could be transmitted to the external block unit. The wireless power transfer is converted into a DC signal with a power rectifier circuit.

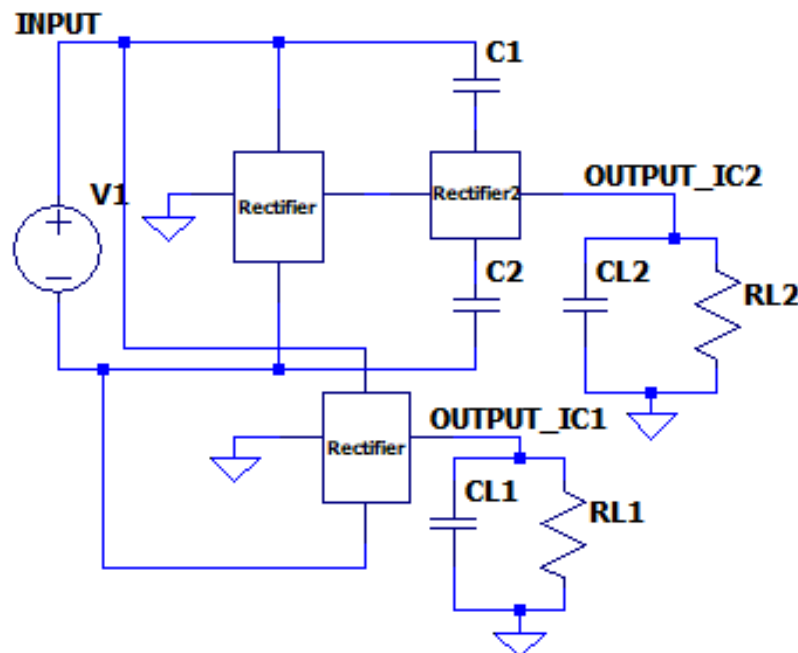
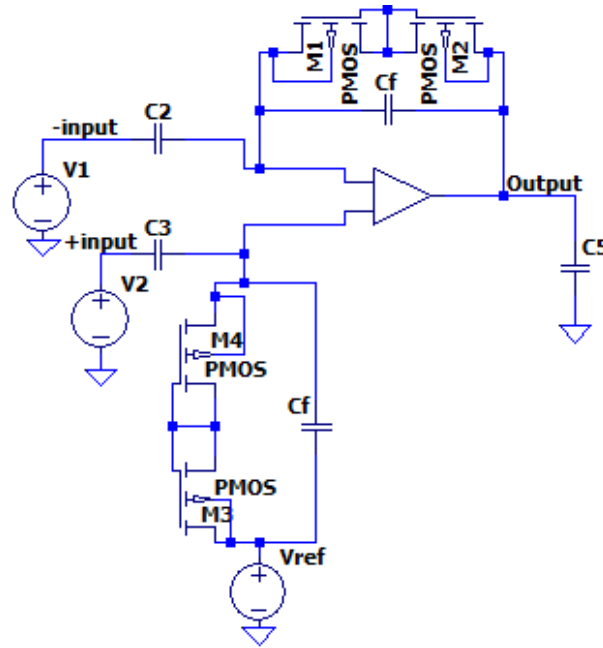


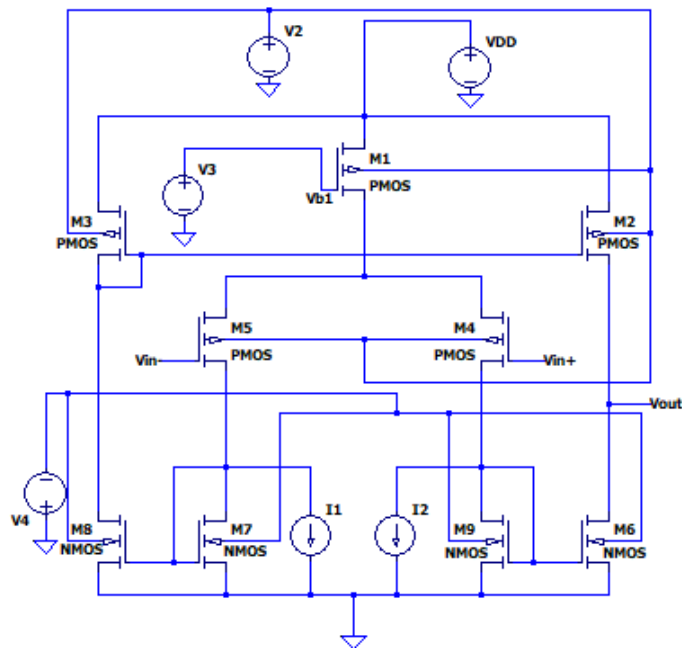
Fig. 2. Typical schematic of an implantable device for neural recording [18]

An implantable device for neural recording contains two integrated circuits (IC's) as shown in Fig. 2[18]: (i) IC1:- It encompasses sensor arrays which gauges neuro-signals and feeds to the neuro-amplifier. The neuro-amplifier amplifies the neuro signal and passes it to subsequent signal processing elements for transmission, and (ii) IC2:- This IC transmits the processed signals. Further, it delivers wirelessly transmitted AC power using the power rectifier (AC-DC converter).

The neuro-amplifier is used for amplification of signals indicating neural activity i.e. action potential and LPF. Gain of the amplifier is determined by the ratio of input capacitance with the feedback capacitance, whereas the bandwidth is controlled by the feedback circuit. The given neuro-amplifier uses current mirror circuitry to increase output resistance for a high open loop gain as shown in Figure 3(a). The operational transconductance amplifier (OTA) with active load (current mirror circuit) takes the input signal as differential input and amplifies the differential signal (Figure 3(b)). OTA is a voltage controlled current source that is used to give high output impedance resulting in a high open loop gain. In order to reduce flicker noise, the gate area of input differential pair can be increased and biased in weak inversion to maximize the g_m/I_D ratio [25]. To minimize the thermal noise effects the rest of the transistors are biased in strong inversion mode.



(a)



(b)

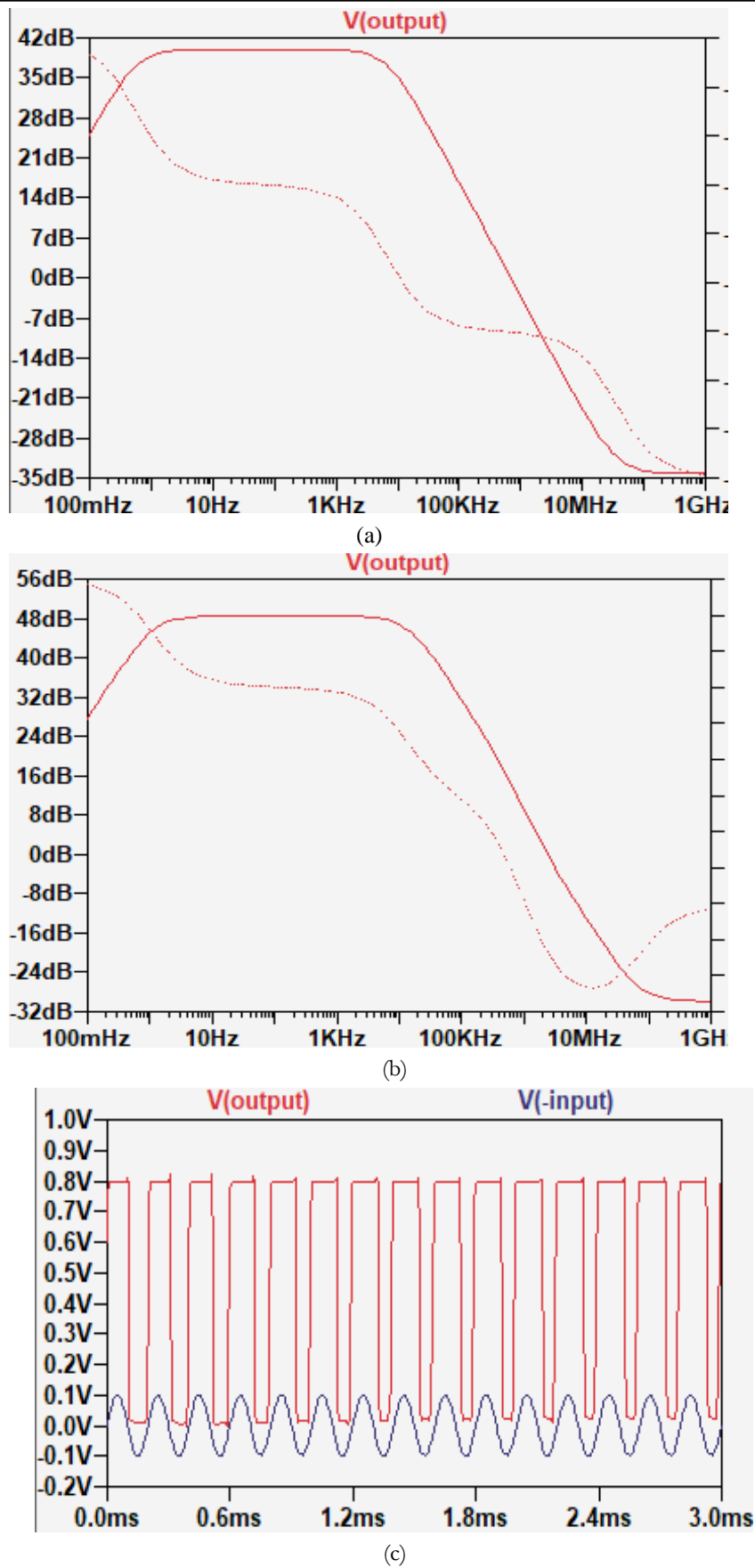


Fig.4. Neuro-amplifier circuit (a) frequency response of original circuit[25], (b) frequency response of the circuit with Miller compensation, and (c) transient response of the OTA.

Table 1: Comparison of the Simulated Neuro Amplifier with the Previous Works

Parameters	Ref [28]	Ref [29]	Ref [30]	Ref [26]	Ref [31]	Ref [32]	Ref [25]	This work*
Technology	1.5 μm	0.180 μm	0.35 μm	0.180 μm	0.5 μm	0.5 μm	0.180 μm	0.180 μm
Supply voltage	3V	1.8 V	3.3V	1.2 V	3 V	2.8 V	0.8V	0.8 V
Power dissipation	115 μW	6.25 μW	23.4 μW	N/A	4.04 μW	7.56 μW	0.8 μW	0.35 μW
Gain	39.3 dB	45.38 dB	73.9 dB	39.2 dB	62 dB	40.9 dB	39 dB	48 dB
Low frequency	0 Hz	5.02 Hz	1 Hz	0.25 Hz	N/A	N/A	1 Hz	1 Hz
High frequency	9.1 kHz	2.927 kHz	10 kHz	28 kHz	4 MHz	N/A	5 kHz	16 kHz
Input referred noise	7.8 μV	1.53 $\mu\text{V}/\text{sqrt}$ (Hz)	1.3 μV	5.79 μV_{rms}	59 nV _{rms} /sqrt (Hz)	1.66 μV_{rms}	0.8 μV_{rms}	N/A

4 Conclusion

This paper elucidates the design and implementation of a neuro-amplifier CMOS OTA circuit using SPICE software. The neuro-amplifier circuit was optimized for gain and bandwidth. Results show that the neuro-amplifier circuit depicts a mid-frequency gain of 48dB, and 3-dB bandwidth of approximately 16 kHz. Circuit optimization and body biasing techniques were implemented to enhance circuit performance metrics.

References

- [1] A. Yakovlev, S. Kim and A. Poon, "Implantable biomedical devices: Wireless powering and communication," *IEEE Communications Magazine*, vol. 50, no. 4, pp. 152–159, 2012.
- [2] K. A. Ng, E. Greenwald, Y. P. Xu and N. V. Thakor, "Implantable neurotechnologies: a review of integrated circuit neural amplifiers," *Med BiolEngComput*, vol. 54, no. 1, pp. 45–62, 2016.
- [3] R. Mathew and A. R. Sankar, "A review on surface stress based miniaturized piezoresistive SU-8 polymeric cantilever platform sensors," *Nano-Micro Letters*, vol. 10, no. 35, 2018.
- [4] R. Mathew and A. R. Sankar, "Design of a triangular platform piezoresistive affinity microcantilever sensor for biochemical sensing applications," *J. Physics D: Applied physics*, vol. 48, p. 205402, 2015.
- [5] R. Mathew and A. R. Sankar, "Impact of isolation and immobilization layers on the electro-mechanical response of piezoresistive nano cantilever sensors," *Journal of Nanoscience and Nanotechnology*, vol. 18, pp. 1636–1647, 2018.
- [6] R. Mathew and A. R. Sankar, "Optimization of a Nano-Cantilever Biosensor for Reduced Self-heating Effects and Improved Performance Metrics," *Journal of Micromechanics and Microengineering*, vol. 28, p. 085012, 2018.
- [7] R. Mathew and A. R. Sankar, "In-Silico investigation of self-heating effects in composite nano cantilever biosensors with integrated piezoresistors," *AIP Advances*, vol. 7, p. 035108, 2017.
- [8] R. Mathew and A. R. Sankar, "Composite silicon dioxide nanocantilever surface stress sensor: design and optimization," *J. Nanosci. Nanotechnol.*, ASP, vol. 18, pp. 3387–3397, 2018.
- [9] R. Mathew and A.R. Sankar, "Influence of surface layer properties on the thermo-electro-mechanical characteristics of a MEMS/NEMS piezoresistive cantilever surface stress sensor." *Materials Research Express* 6, no. 8 (2019): 086304," *Materials Research Express*, vol. 6, no. 8, p. 086304, 2019.
- [10] R. Mathew and A. R. Sankar, "Temperature drift-aware material selection of composite piezoresistive micro-cantilevers using Ashby's methodology," *Microsystem Technologies*, pp. 1–14, 2020.

- [11] R. Mathew and A. R. Sankar, "Numerical study on the influence of buried oxide layer of SOI wafers on the terminal characteristics of a micro/nano cantilever biosensor with an integrated piezoresistor," *Biomedical Physics & Engineering Express*, vol. 2, no. 5, p. 055012, 2016.
- [12] R. Mathew, K. Nag, A. Sharma, A. Krishna and S. Sathvik, "Material and Geometry Selection of a Multi-layer Microcantilever Thermal Sensor with Piezoresistive Readout," in Second International Conference on Applied physics, Power and Material Science (APPM) Secunderabad' 19, 2019.
- [13] K. V. Meena and R. Mathew, "Performance comparison of single element piezoresistors with a half-active Wheatstone bridge for miniaturized pressure sensors," *Measurement*, vol. 111, pp. 340–350, 2017.
- [14] K. V. Meena and Ribu Mathew, "Design and optimization of a three terminal piezoresistive pressure sensor for catheter based in-vivo biomedical applications," *Biomedical Physics & Engineering Express*, vol. 3, p. 045003, 2017.
- [15] Q. Xu, T. Wang, S. Mao, W. Jia, Z. H. Mao and M. Sun, "Wireless Power Transfer for Miniature Implantable Biomedical Devices," *Wireless Energy Transfer Technology*, 2019.
- [16] D. Ahn and S Hong, "Wireless power transmission with self-regulated output voltage for biomedical implant," *IEEE Transactions on Industrial Electronics*, vol. 61, no. 5, pp. 2225–2235, 2013.
- [17] Hashemi, S. Saeid, M. Sawan, and Y. Savaria, "A high-efficiency low-voltage CMOS rectifier for harvesting energy in implantable devices," *IEEE Transactions on Biomedical Circuits and Systems*, vol. 6, no. 4, pp. 326–355, 2012.
- [18] H. K. Cha and M. Je, "A single-input dual-output 13.56 MHz CMOS AC–DC converter with comparator-driven rectifiers for implantable devices," *Microelectronics Journal*, vol. 45, no. 3, pp. 277–281, 2014.
- [19] M. Joshi, R. Mathew, P. Sarkar, A. Dutta, S. Tiwari and P. Nigam, "Performance Analysis of Radio Frequency (RF) Low Noise Amplifier (LNA) with various Transistor Configurations," in IEEE international conference ICDCS 2020, 2020.
- [20] P. Manikandan and Ribu Mathew, "Design of a CMOS class-E power amplifier for WLAN and blue tooth applications," in IEEE international conference ICDCS 2012, 2012.
- [21] P. C. Crepaldi, L. H. de C. Ferreira T. C. Pimenta R. L. Moreno L. B. Zoccal and E. C. Rodriguez, "Structural Design of a CMOS Voltage Regulator for an Implanted Device," *Current trends and challenges in RFID*, 2011.
- [22] U. Bihl, T. Ungru, H. Xu, J. Anders, J. Becker and M. Ortmanns, "A bidirectional neural interface with a HV stimulator and a LV neural amplifier," *IEEE International Symposium on Circuits and Systems*, pp. 401–404, 2013.
- [23] A. Banuaji and H. K. Cha, "A 15-V bidirectional ultrasound interface analog front-end IC for medical imaging using standard CMOS technology," *IEEE Transactions on Circuits and Systems II: Express Briefs*, vol. 61, no. 8, pp. 604–608, 2014.
- [24] R. Shulyzki, K. Abdelhalim, A. Bagheri, M. T. Salam, C. M. Florez, J. L. P. Velazquez, P. L. Carlen and R. Genov, "320-channel active probe for high-resolution neuromonitoring and responsive neurostimulation," *IEEE transactions on biomedical circuits and systems*, vol. 9, pp. 34–49, 2014.
- [25] A. Abdi and H. K. Cha, "A bidirectional neural interface CMOS analog front-end IC with embedded isolation switch for implantable devices," *Microelectronics journal*, vol. 58, pp. 70–75, 2016.
- [26] H. S. Kim and H. K. Cha, "A low-noise biopotential CMOS amplifier IC using low-power two-stage OTA for neural recording applications," *Journal of Circuits, Systems and Computers*, vol. 27, no. 5, p. 1850068, 2018.
- [27] U. Bihl, J. Anders, J. Rickert, M. Schuettler, A. Moeller, K. H. Boven, J. Becker and M. Ortmanns, "A neural recorder IC with HV input multiplexer for voltage and current stimulation with 18 V compliance," *IEEE European SolidState Circuits Conference*, pp. 103–106, 2014.
- [28] P. Mohseni, and K. Najafi "A low power fully integrated bandpass operational amplifier for biomedical neural recording applications," in *Proceedings of the Second Joint EMBSIBMES Conference*, 2002, pp. 1845–1853.
- [29] K Pratyusha, S Kumar and A Kumari, "Low power amplifier for biopotential signal acquisition system," in *ICACCI 2015*, 2015, pp. 324–329.
- [30] Joseph N. Y. Aziz, Roman G., Berj L.B. et al., "Brain-Silicon Interface for high-Resolution in vitro neural recording," *IEEE Trans. on Biomedical Circuits and Systems*, vol. 1, no. 1, pp. 56–62, 2007.
- [31] S. Shirin Saberhosseini, A. Zabihiyan, and Amir M. Sodagar, "Low-Noise OTA for Neural Amplifying Applications," in *2012 8th International Caribbean Conference on Devices, Circuits and Systems (ICDCS)*, 2012, pp. 1–4.
- [32] W. Wattanapanitch, M. Fee, and R. Sarpeshkar, "An energy-efficient micropower neural recording amplifier," *IEEE transactions on biomedical circuits and systems*, vol. 1, no. 2, pp. 136–147, 2007.